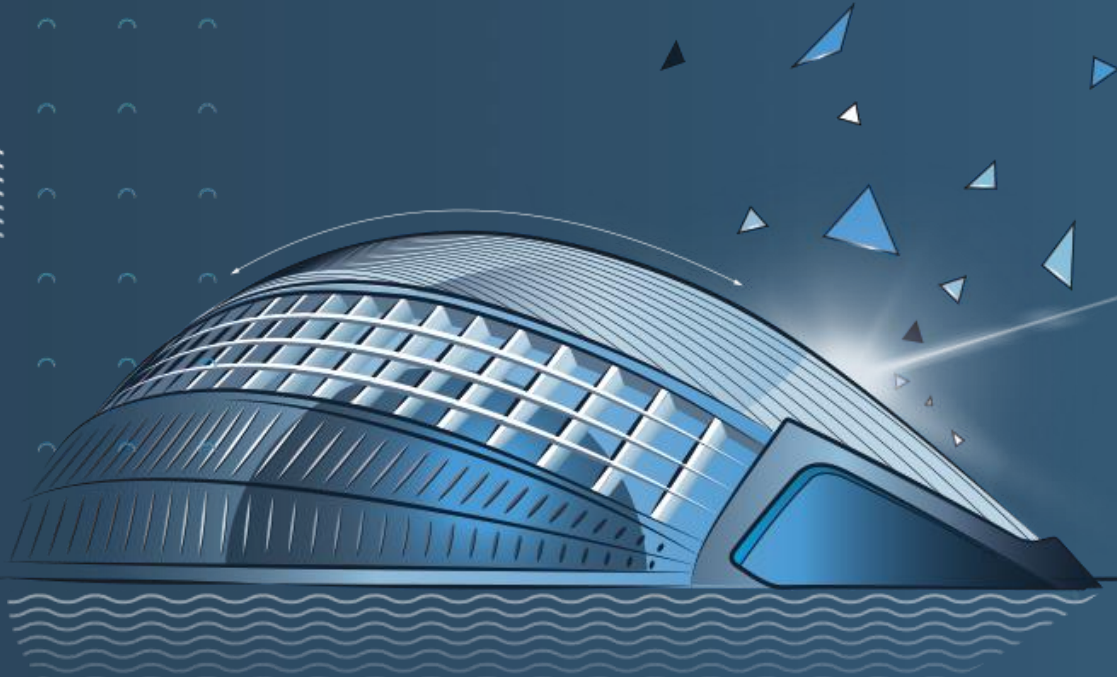


sense

Spine Expert NetworkTM
for Science & Education



Controlling forces in trauma indications: How to get the best of the technique

SENSE

2nd International
Spine Expert Symposium

June 23 – 25, 2022 / Valencia – Spain

Dr. Patrick A. Weidle



Principle of Fracture Treatment:

A) Reposition

B) Stabilisation

C) Holding of the Stabilisation



Energy vs. Bone Quality



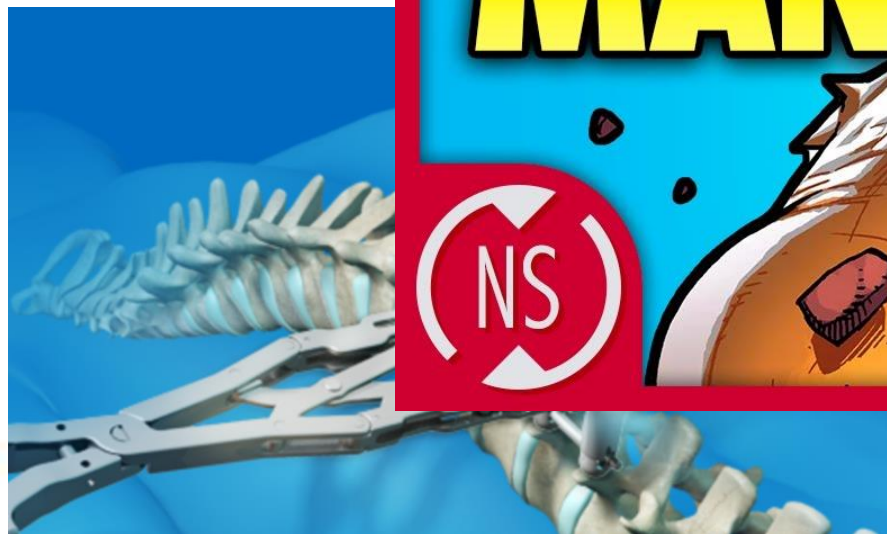
Germany: 80% of the VBF are patients with poor bone quality!

Positioning of the Patient = Repositioning of the Fracture via Ligamentotaxis





POWER MAN?



Reasons for Revision Surgery – Implant Failure



www.spine-deformity.org

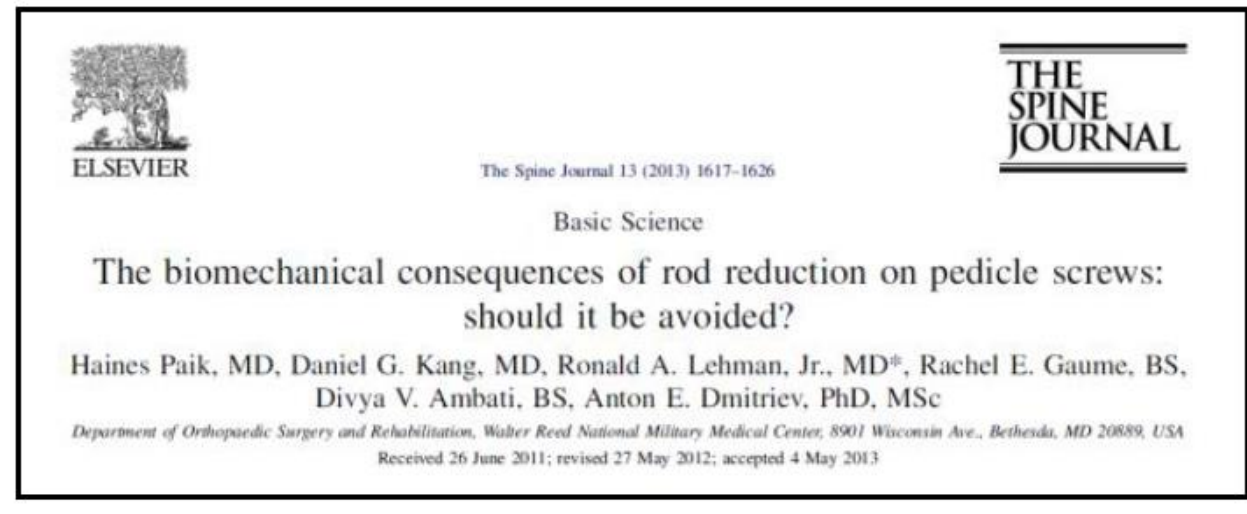
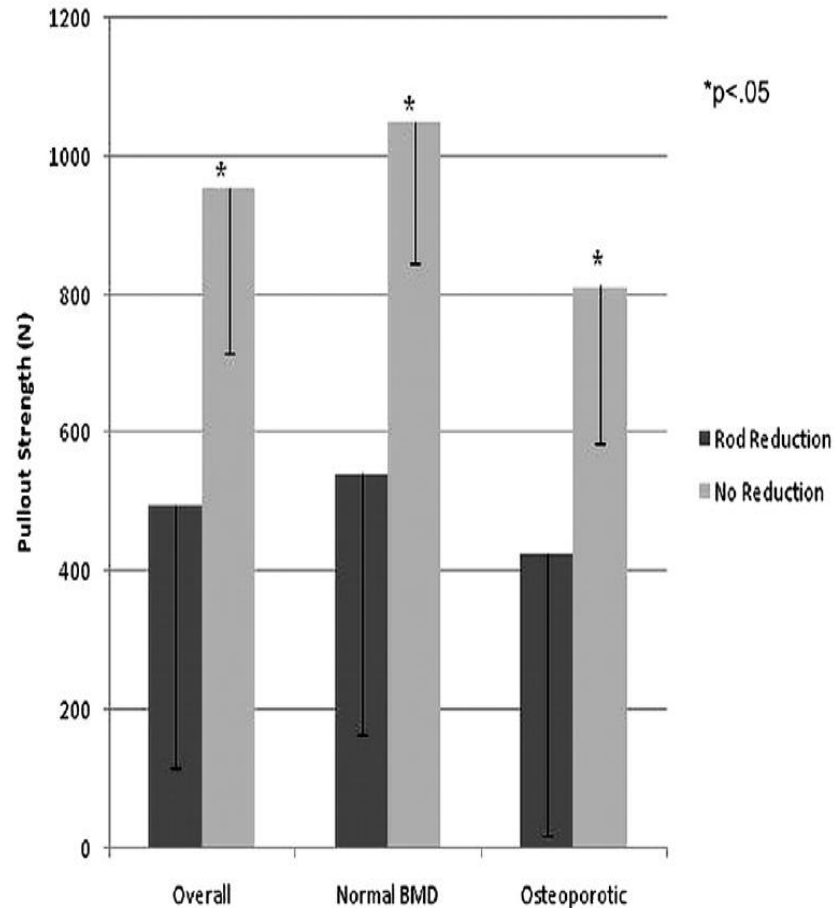
Spine Deformity xx (2019) 619–626

Revision Risk After Primary Adult Spinal Deformity Surgery:
A Nationwide Study With Two-Year Follow-up

Frederik T. Pitter, MD^{a,*}, Martin Lindberg-Larsen, MD, PhD^b,
Alma B. Pedersen, MD, PhD, DMSc^c, Benny Dahl, MD, PhD, DMSc^d,
Martin Gehrchen, MD, PhD^a

Reasons for revision in the 110 patients.	
Reasons	n (%) (95% CI)
Implant failure	42 (38.2)
Infection	13 (11.8)
Curve progression	12 (10.9)
Pseudarthrosis	12 (10.9)
Neurologic deficit	12 (10.9)
Other	9 (8.2)
PJK	8 (7.3)
Unknown	2 (1.8)

Clinical Outcomes – Screw Loosening



48% reduced bone anchorage/biomechanical fixation strength after attempted reduction using a persuasion device

5-mm-reduction is enough to cause screw loosening

Try to avoid reduction using a persuasion device (osteoporosis)!

1. Kang DG, et al. Effects of rod reduction on pedicle screw pullout strength in osteoporotic bone.

Clinical Outcome – Screw Loosening

ORIGINAL ARTICLE

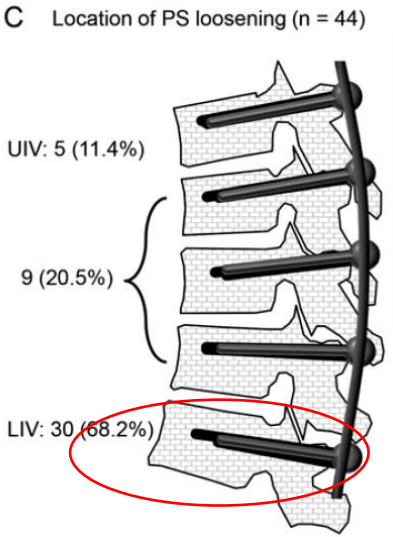
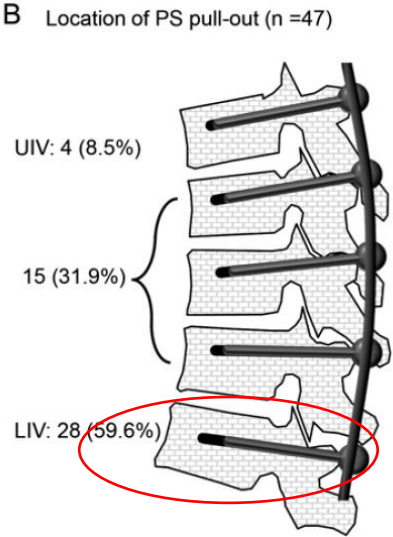
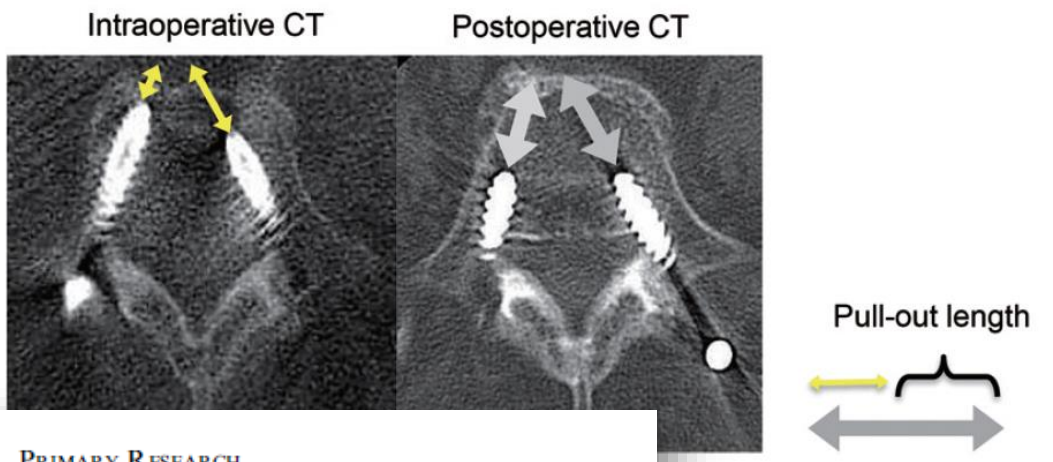
SPINE SURGERY AND RELATED RESEARCH

Risk Factors for Clinically Relevant Loosening of Percutaneous Pedicle Screws

Tetsuro Ohba¹⁾, Shigeto Ebata¹⁾, Hiroki Oba^{1,2)}, Kensuke Koyama¹⁾ and Hirofuka Haro¹⁾

1) Department of Orthopaedic Surgery, University of Yamanashi, Chuo-city, Japan
2) Department of Orthopaedic Surgery, Shinshu University, School of Medicine, Matsumoto-city, Japan

15% - 16% Screw Loosening & Screw Pull-out Rate



PRIMARY RESEARCH

Utility of a Computer-assisted Rod Bending System to Avoid Pull-out and Loosening of Percutaneous Pedicle Screws

82% of loosened screws were pulled out during final rod connection!

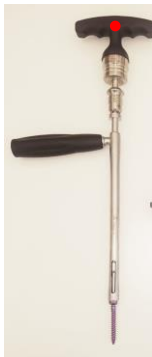
48% less screw loosening in computer assisted rod bending!

Forced Fixation ? – A problem of design?

Heavy Instruments with a high physical center (bad lever!)

Weight: ~0.8 kg - 1.5 kg.
reduce the tactile feeling

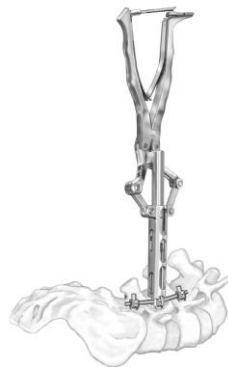
Bad Lever:
~70% topeavy
~ 35% longer
~40x more mechanical stress



Instruments block polyaxiality

Position of the screw head:
Prohibit the perpendicular alignment
Screw - Rod

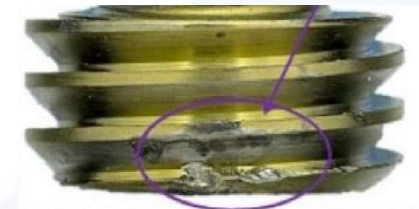
Reduction power: pulls the spine to the rod – bad anatomical load!



Flat Set Screws

Flat Design: Limited perpendicular alignment – last ½ turn!

Friction: Cold welding – Failure of the stabilisation



Principles of Controlled Fixation

1

**Anatomical Screw
Head Position**



*The Screwheads
always bring into
reproducible unforced
line, when bringing in
the rod*

2

**Keep the Screw Head
polyaxial**



*Everything which is
blocking the
Polyaxiality
(Instruments,
Anatomy) causes bad
loads*

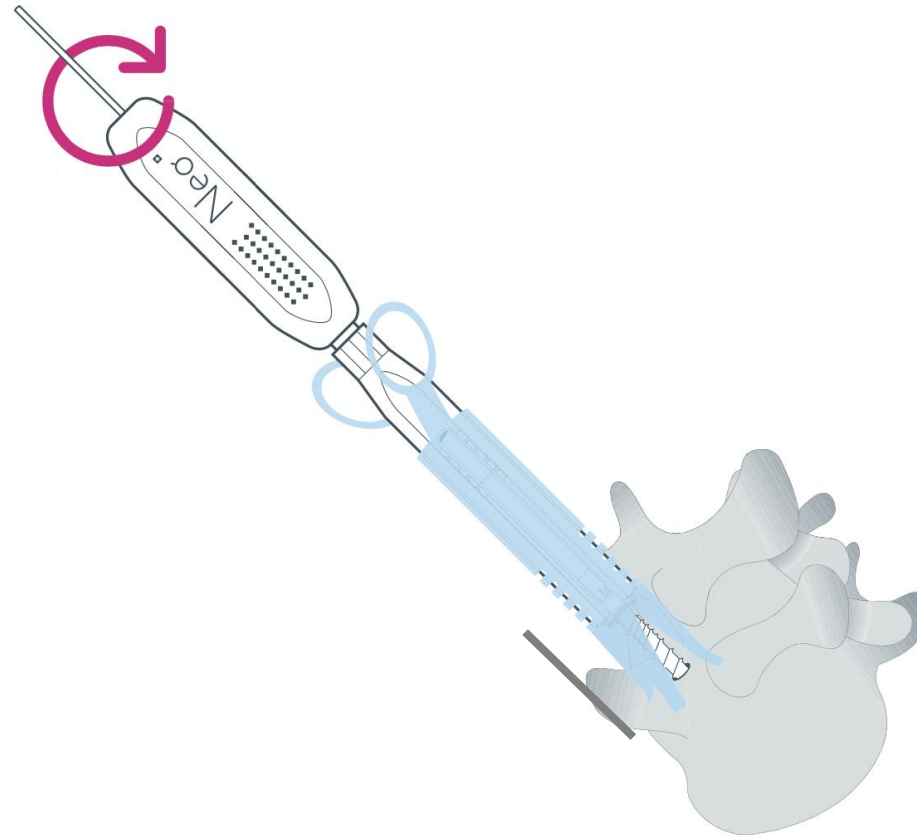
3

**Controll of the
mechanical forces**



*The system should give
a feedback to identify
and controll
mechanical loads*

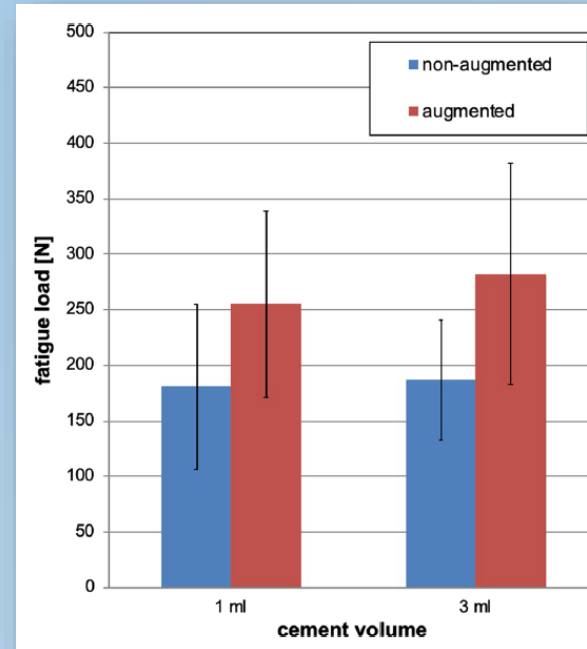
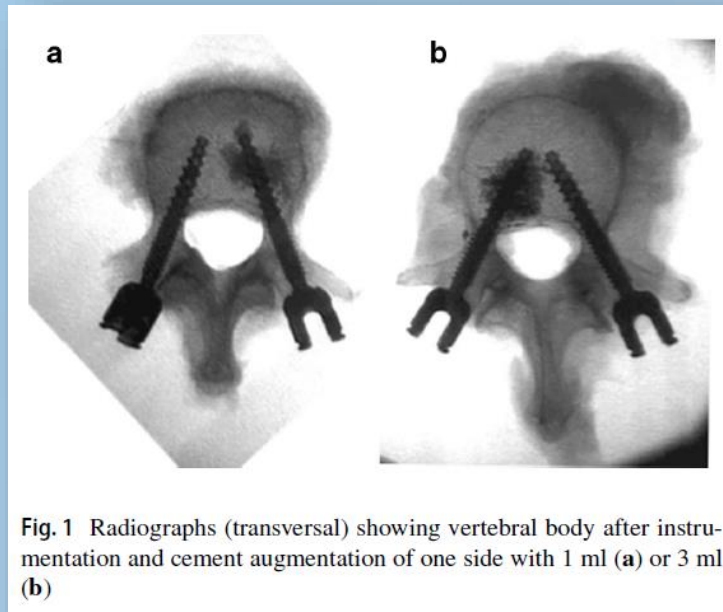
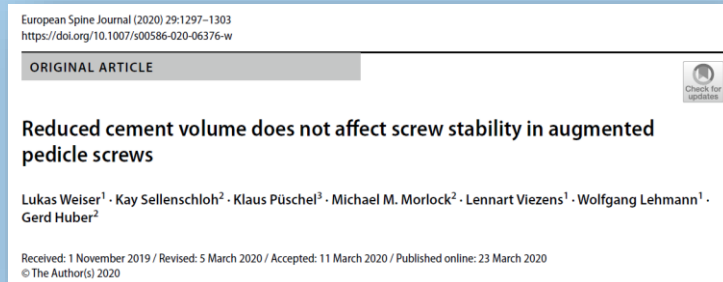
Implantation of the Screw



CONTROLLED FIXATION DESIGN

- K-Wire and lighth screwdriver for navigation of the screw
- Short lever
- No need of drilling a thread

Cement Augmentation



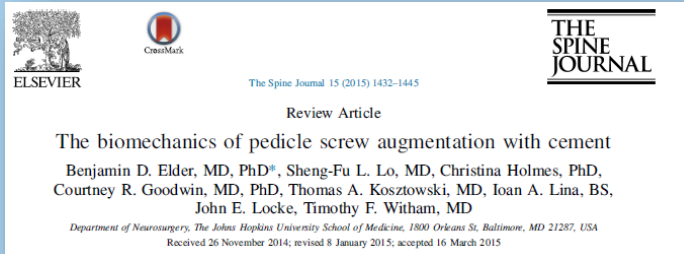
Compared to the non-augmented screws, augmentation with:

- 1 ml bone cement increased the fatigue load by 41%
- 3 ml increased the fatigue load by 51%

There was no significant difference in fatigue loads between the specimens with screws augmented with 1 ml and screws augmented with 3 ml of bone cement ($p = 0.504$).

“A spare usage of bone cement (around 1 ml) for each pedicle screw appears to be recommendable”

Cement Augmentation



■ Systematic Literature Review

CONCLUSION

PMMA along with several calcium ceramic materials, are effective materials for enhancing pedicle screw fixation.

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Table 2
Biomechanical testing of PMMA screw augmentation with fenestrated or cannulated screws

Study	Subject	Levels	Fixation material	Screw and cement implantation	Volume (cc)	Screw insertion time (min)	Biomechanics	Results	Failure mode	Comments
Becker et al. [12]	Cadaveric spines	L1–L4	PMMA	Solid, fenestrated, vertebroplasty vs. kyphoplasty	2	6	Axial pullout	1.5- to 1.8-fold increase in pullout strength with cement, no difference between fenestrated screw, vertebroplasty, or kyphoplasty	Screw stripping for fenestrated screw, bone-cement interface for solid screws	Epidural cement leakage with fenestrated screw
Chao et al. [13]	Osteoporotic cadaveric spines	T10–L5	PMMA	Fenestrated (prefilled or through screw)	2	0	Axial pullout, stiffness, energy to failure	4- to 5.6-fold increase in pullout strength with cement, prefilling hole with higher failure energy than injecting through fenestration	Bone-cement interface	Injecting through fenestrated screw with cement only at distal end of screw where fenestration located
Goost et al. [14]	Normal vs. osteoporotic cadaveric vertebrae	T12–L5	PMMA	Fenestrated, with or without cement	3	NR	Axial pullout	2.1-fold increase in pullout strength for osteoporotic group, 1.5-fold increase in normal group	NR	No cement extravasation
Chen et al. [15]	Synthetic bone blocks simulating severe osteoporosis	NA	PMMA	Solid vs. fenestrated, conical vs. cylindrical	3	1	Axial pullout	Prefilling cement had improved pullout strength compared with fenestrated screw injection	Bone-cement interface	Enhanced initial fixation, no loss of fixation strength when backing screws out 360°
Chen et al. [16]	Synthetic bone	NA	PMMA	Fenestrated screw, with or without radial holes	3	1	Axial pullout	Pullout strength increased with greater number of radial screw holes	Bone-cement interface	Cement exuded primarily from proximal holes
Waits et al. [17]	Osteopenic cadaveric vertebrae	L1–L5	PMMA	Fenestrated, left in place or replaced before curing	2.5	0	Cephalocaudal toggle displacement, removal torque	63% motion reduction for cemented screws	NR	Removal torque 10-fold higher if fenestrated screw left in place after cement injection
Kueny et al. [18]	Osteoporotic cadaveric vertebrae	L1–L5	PMMA	Fenestrated, prefilled, screw-injected, large diameter nonaugmented	NR	NR	Toggle fatigue testing, axial pullout	Both cement augmentation techniques increased pullout force, but better fatigue resistance in screw-injected group	NR	Cement leakage in 6 of 9 vertebrae
Choma et al. [19]	Osteoporotic cadaveric vertebrae	T6–L5	PMMA	Nonaugmented, solid with PMMA, partially fenestrated, fully fenestrated	2	NR	Axial pullout, removal torque	All augmentation techniques significantly better pullout strength than control; partial fenestration had better pullout strength than solid screw with cement prefilling	Screw-cement interface during removal	No difference in pullout strength between high- and low-viscosity cement, no difference in extraction torque for solid screws or fenestrated screws, no vertebral body damage with removal

NA, not applicable; NR, not recorded; PMMA, polymethylmethacrylate.

Cement Augmentation

Eur Spine J (2014) 23:2196–2202
DOI 10.1007/s00586-014-3476-7

ORIGINAL ARTICLE

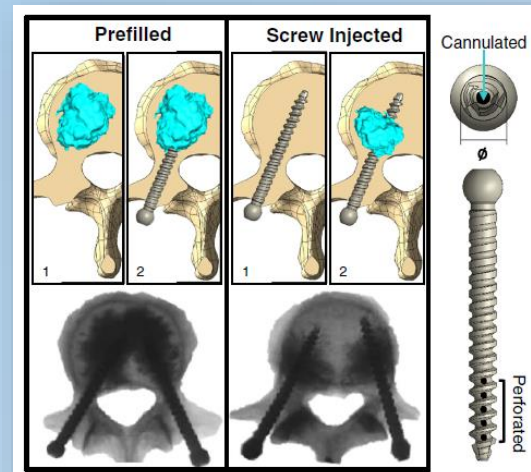
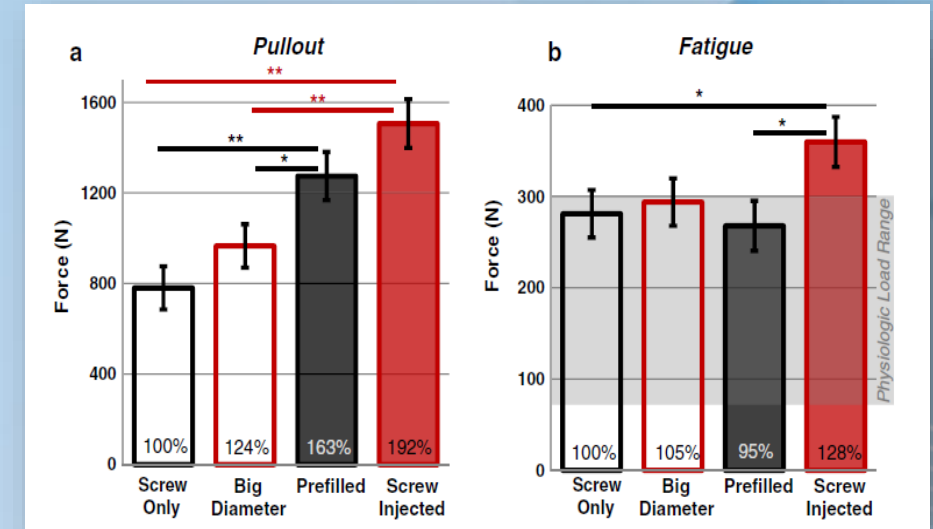
Influence of the screw augmentation technique and a diameter increase on pedicle screw fixation in the osteoporotic spine: pullout versus fatigue testing

Rebecca A. Kueny · Jan P. Kolb · Wolfgang Lehmann ·
Klaus Püschel · Michael M. Morlock ·
Gerd Huber

- Biomechanical study in human osteoporotic cadaveric spine
- 39 lumbar vertebrae
- To determine the fixation strength of current fixation techniques

4 treatment groups:

- screw only (control)
- non-augmented, increased diameter
- prefilled augmentation
- screw injected augmentation



- Screw injected augmentation showed the best biomechanical stability.
- Key for achieving stable screw fixation in the osteoporotic spine:

Utilizing screw injected cement augmentation along with a maximal screw diameter.

REVIEW ARTICLE

Pedicle screw fixation of thoracolumbar fractures: conventional short segment versus short segment with intermediate screws at the fracture level—a systematic review and meta-analysis

Carolijn Kapoen¹  · Yang Liu² · Frank W. Bloemers¹ · Jaap Deunk¹

Systematic review: 21 randomized controlled trials with a total of 1890 patients

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Significantly

- lower pain scores
- better short- and long-term Cobb angles
- less loss of correction
- less implant failures

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Significantly

- lower pain scores
- better short- and long-term Cobb angles
- less loss of correction
- less implant failures

Significantly

- longer operation time
- more blood loss



Article

Efficacy and Radiographic Analysis of Minimally Invasive Posterior Mono-Axial Pedicle Screw Fixation in Treating Thoracolumbar Burst Fractures

Jae-Hoon Shim and Eun-Min Seo * 

Department of Orthopedic Surgery, Chuncheon Sacred Heart Hospital, Hallym University College of Medicine, Chuncheon 24253, Korea; shim0121@hallym.or.kr

* Correspondence: seoem@hallym.or.kr; Tel.: +82-33-240-5198

Randomized controlled trial with a total of 98 patients; mono-axial vs. poly-axial
Traumatic fractures; healthy bone quality

Mono-Axial PS-Fixation was significantly better in correction of regional angle of kyphosis and maintaining anterior vb height

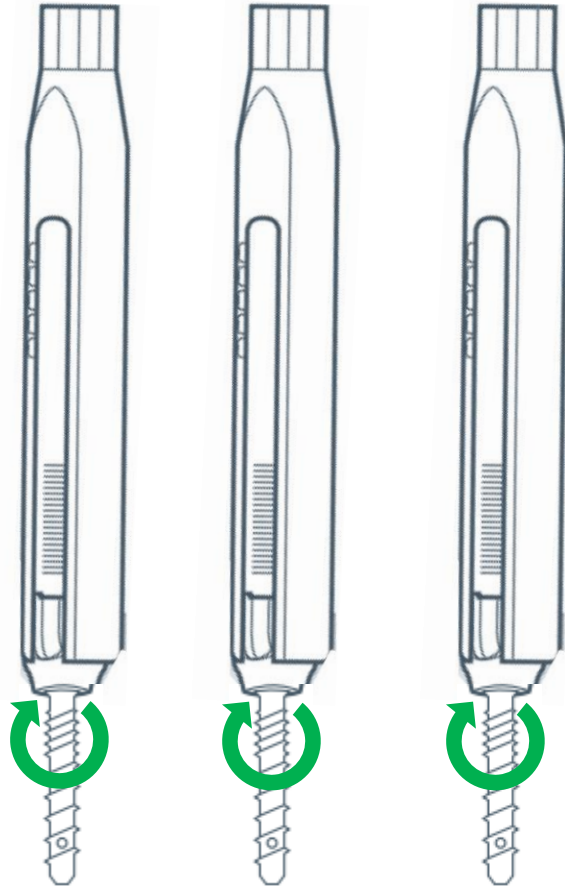
MO-PS Correction of path. Kyphosis: 62%

Loss of Correction after 12 Mo: 15%

PA-PSD Correction of path. Kyphosis: 52%

Loss of Correction after 12 Mo: 33%

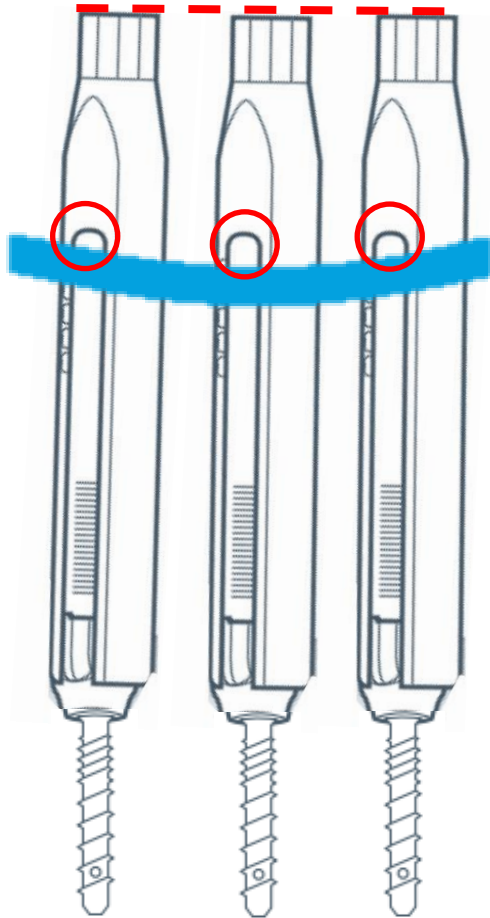
Polyaxiality of the screws



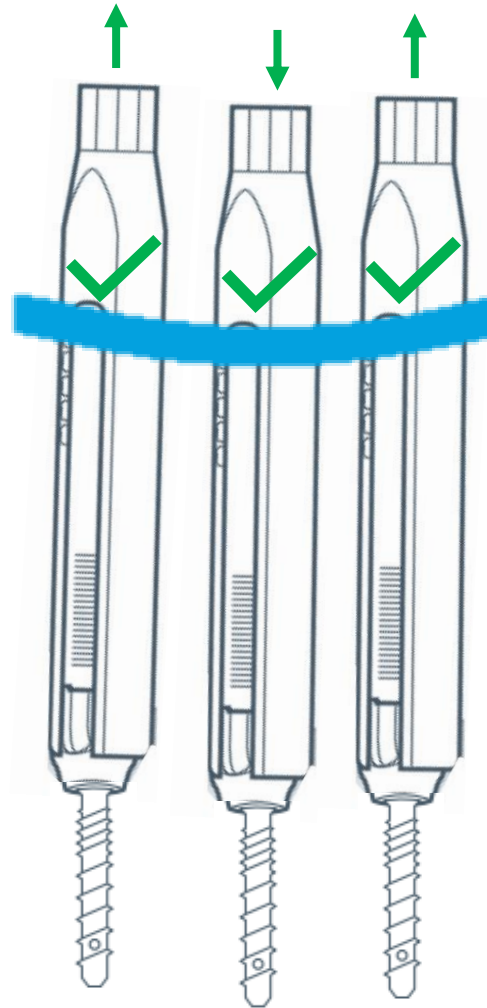
CONTROLLED FIXATION DESIGN

- GuideTower: Enables to ensure polyaxiality

Modification of the rod (or of the screws!?)



Misalignment screw - rod



Perfect Alignment screw – rod!
Controlled Fixation!

CONTROLLED FIXATION DESIGN

- Inspection of the height of the guide tower
- Inspection of length and bending of the rod at the domes of the guide



Consequence

- Visuell confirmation of an expected perfect fit of the rod to the screws (Avoidance of bad mech. Loads)
- Visuell controll of reduction at any time point

Pre-Fixation of the rod & Torque limiter



CONTROLLED FIXATION DESIGN

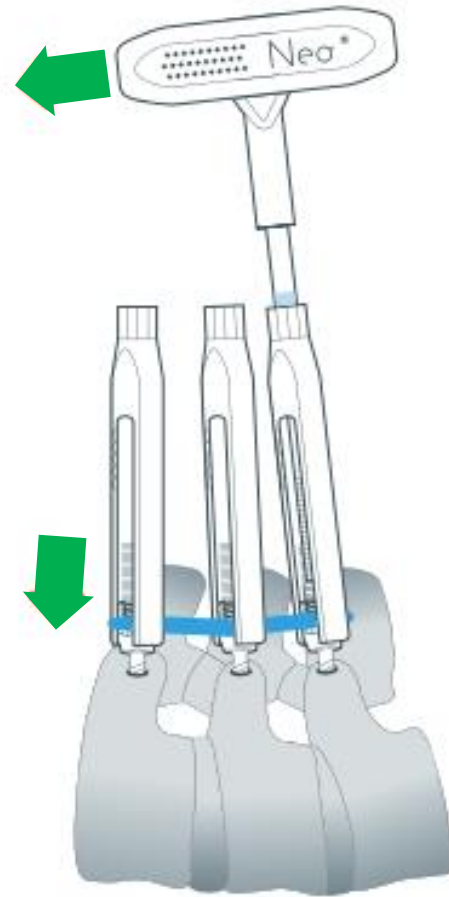
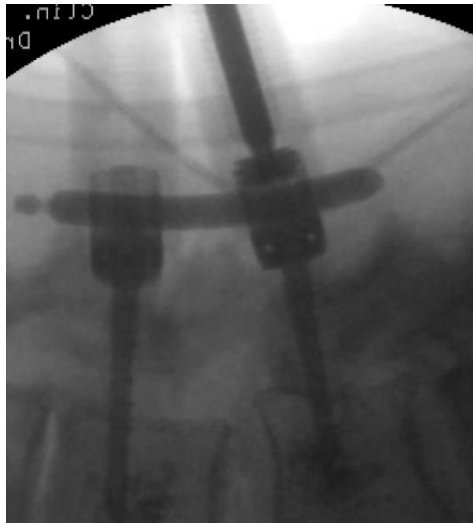
- Light removable rod holder
- Torque limiter to avoid rod migration



Consequence

- Preservation of mobility
- Reduction of tissue damage because of the early removing of the rod holder

Stressless positioning of the rod



CONTROLLED FIXATION DESIGN

- Rod reduction via polyaxiality of the screw heads
- Segmental removal of the guide towers



Effect: Controlled Fixation

- No uncontrolled forces while bringing in the rod to the screw heads
- Full control of the rod-position to achieve a specific correction

Locking the set screw

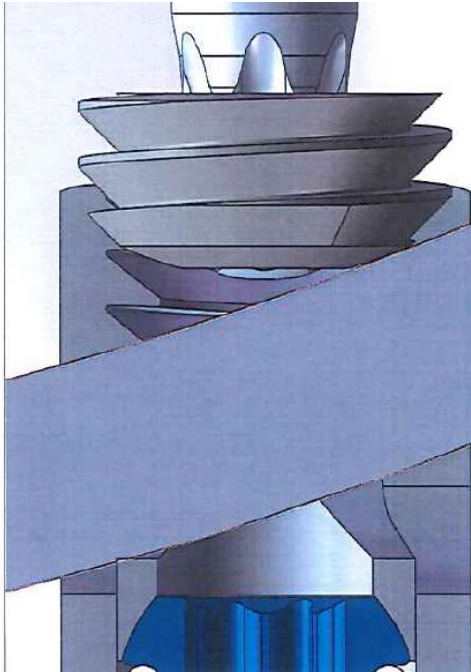


Figure 7 [1] Rod / set screw contact



CONTROLLED FIXATION DESIGN

- Light guide tower
- Convex set screw
- Prominet StainlessSteel-Torx – 'frictionless' locking



Effect: Controlled Fixation

- Mobility enables the perfect perpendicular adaption of the implants interface
- Reduced cold welding
- Reduced implant failure

Locking the set screw

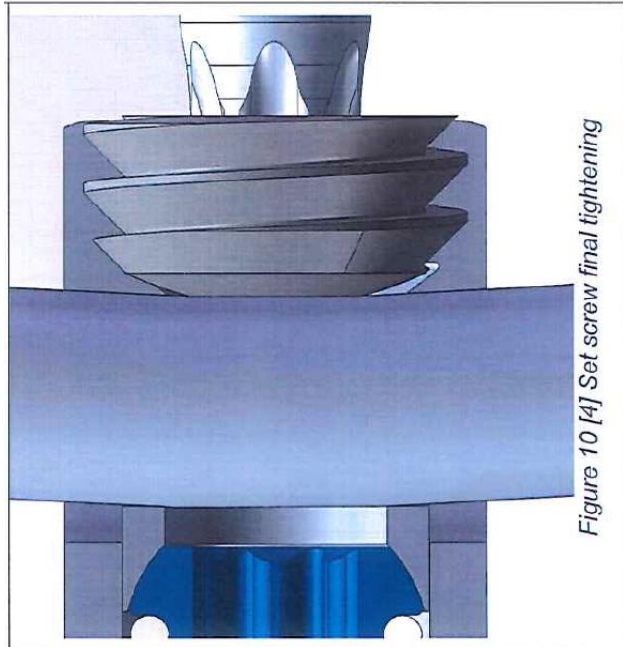


Figure 10 [4] Set screw final tightening



CONTROLLED FIXATION DESIGN

- Light guide tower
- Convex set screw
- Prominet StainlessSteel-Torx – 'frictionless' locking



Effect: Controlled Fixation

- Mobility enables the perfect perpendicular adaption of the implants interface
- Reduced cold welding
- Reduced implant failure

Locking the construct



!!! Attention – Think different !!!

REDUCTION/LOCKING:

- PARALLEL
- SYMETRIC
- ALTERNATING
- SEGMENTAL Removal of the Guide Towers

→ Effect: Controlled fixation

Avoidance of:

- Coronal Deformation
- Sagittal Compression / Distraction
- Mal-Rotation



Patrick A. Weidle
Head of Department
Muskulo-Skeletal
Center
Spine Center
Krankenhaus Neuwerk
Mönchengladbach



Thank you for your attention!



CR I:

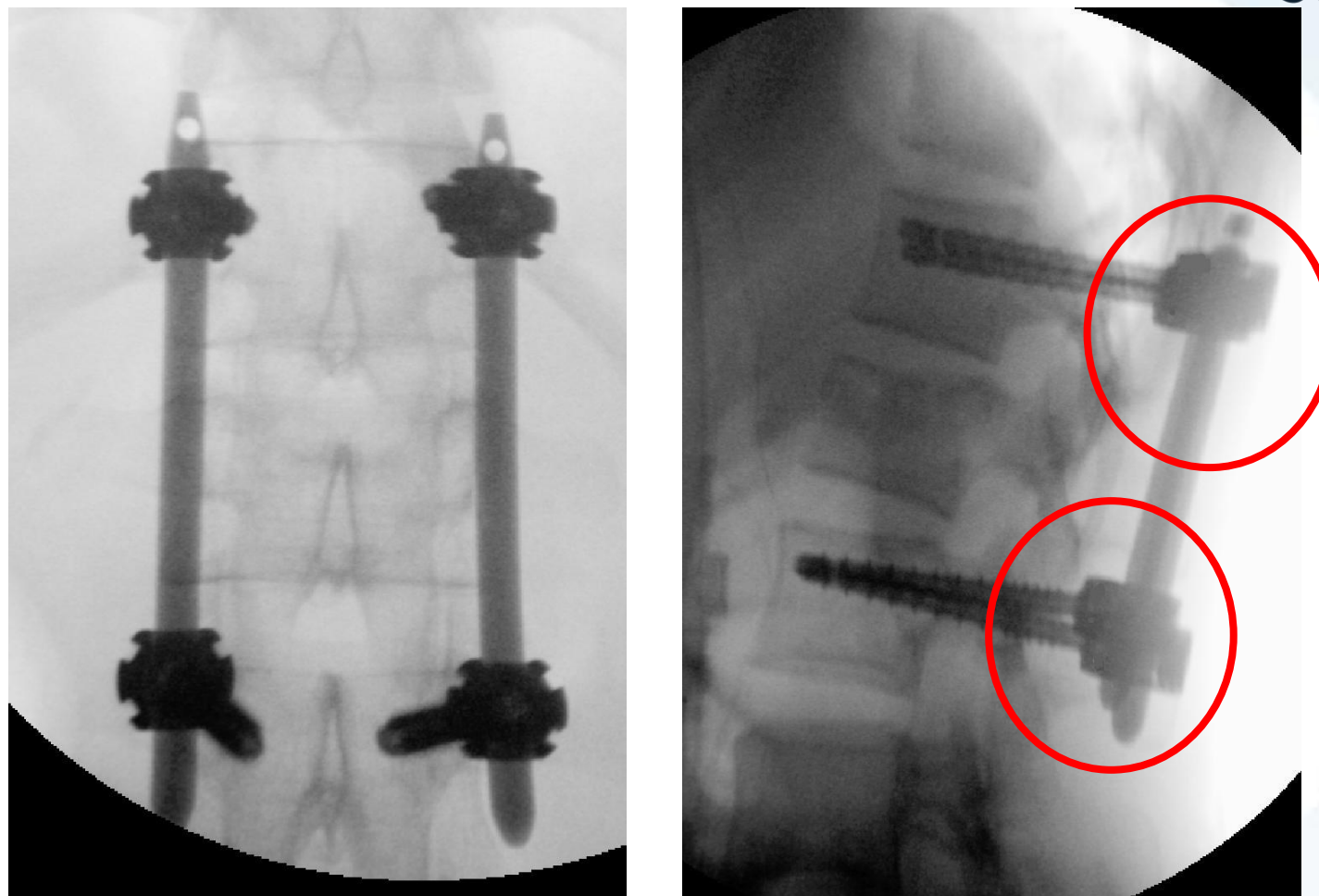
High-Energy-Traum, Healthy Bone Qual.

Male, 28 LY, no secondary diagnosis

Unstable L1-Burst-Fracture







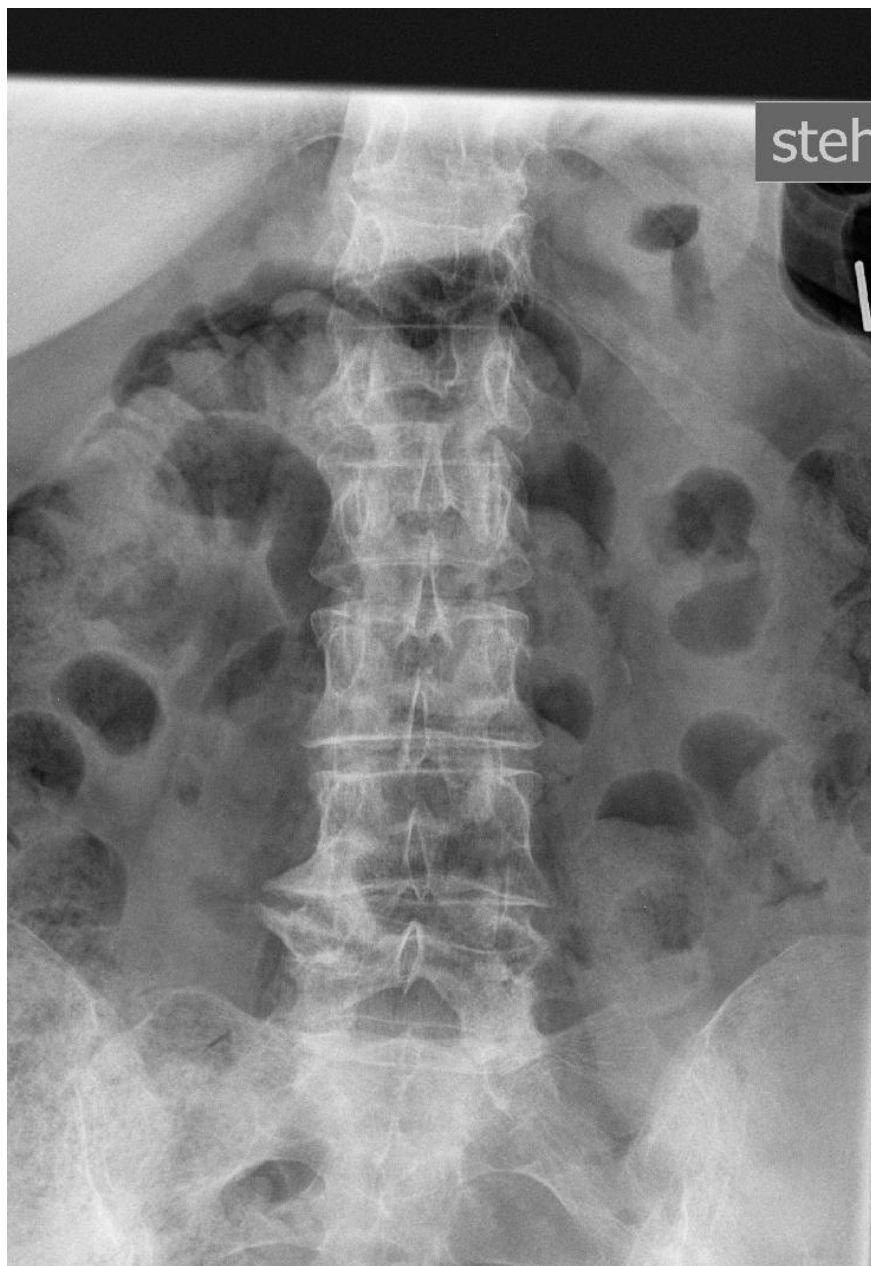
Reposition via hyperlordotic Positioning of the Patient and Ligamentotaxis
+
Monoaxial Screws

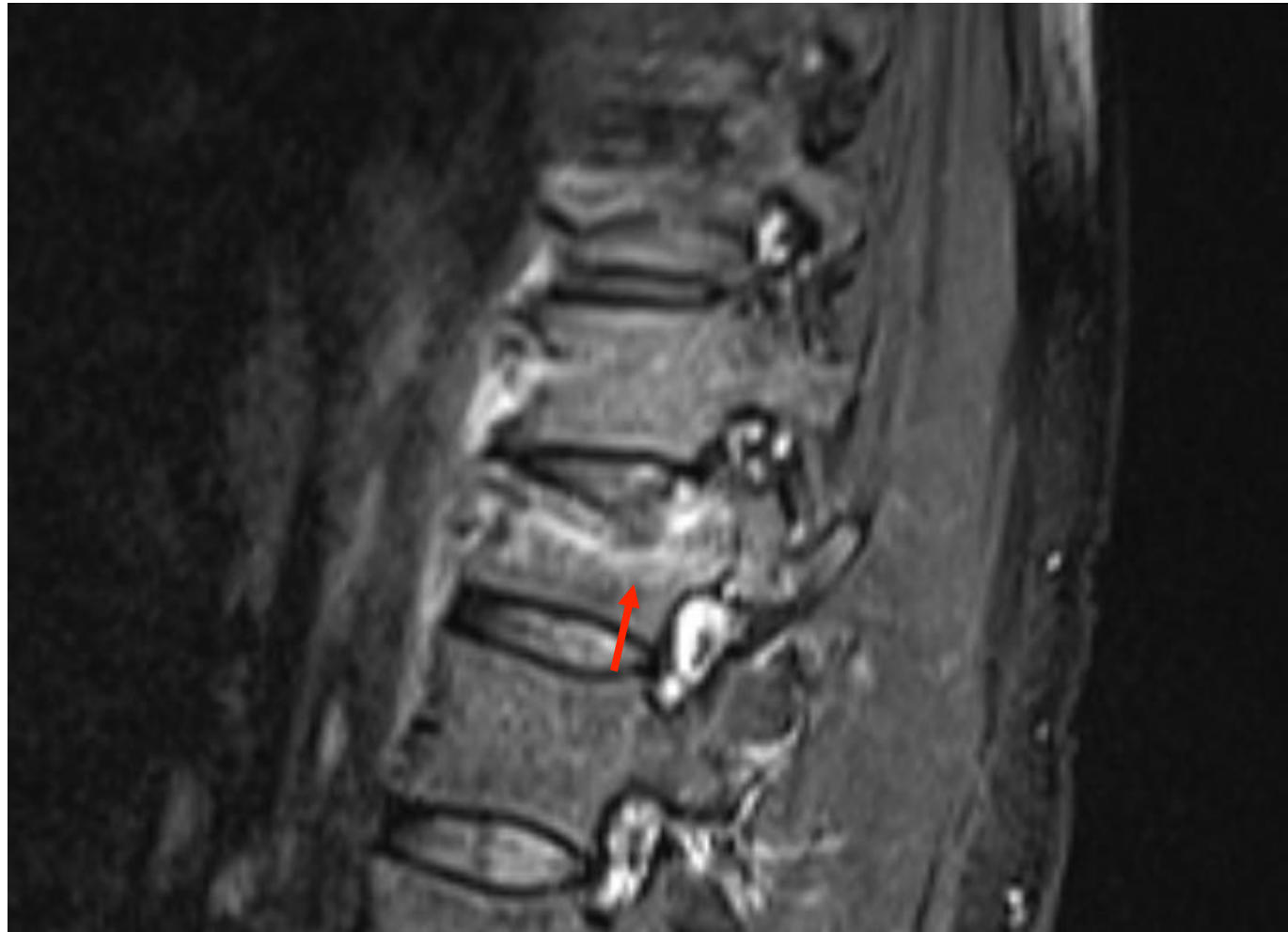
CR II:

High-Energy-Traum, Healthy Bone Qual.

Female, 41 LY, no secondary diagnosis

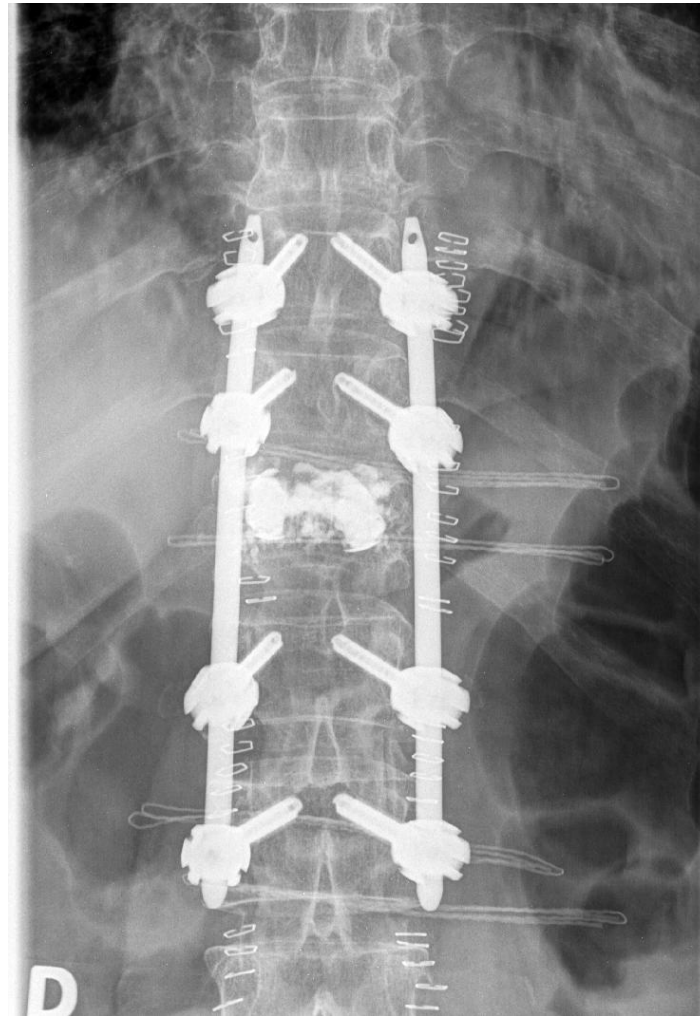
Unstable T12-Burst-Fracture with Disc-Tear-Drop and PF





VB-Replacement???

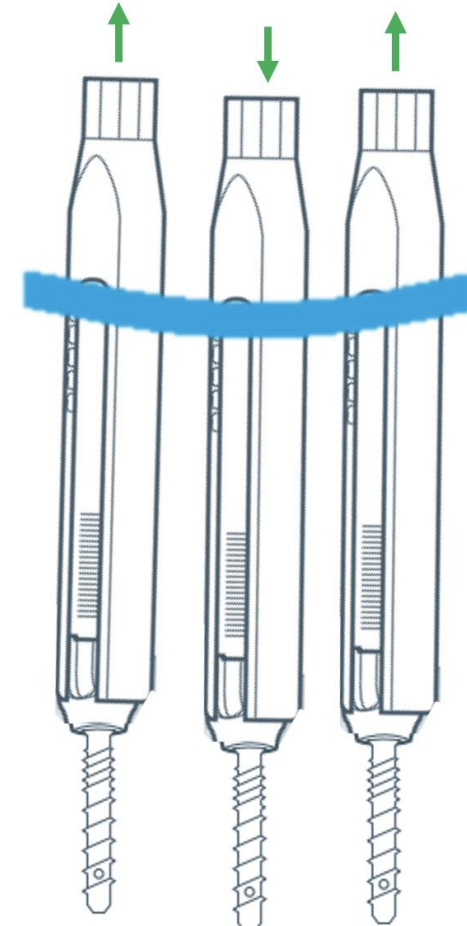
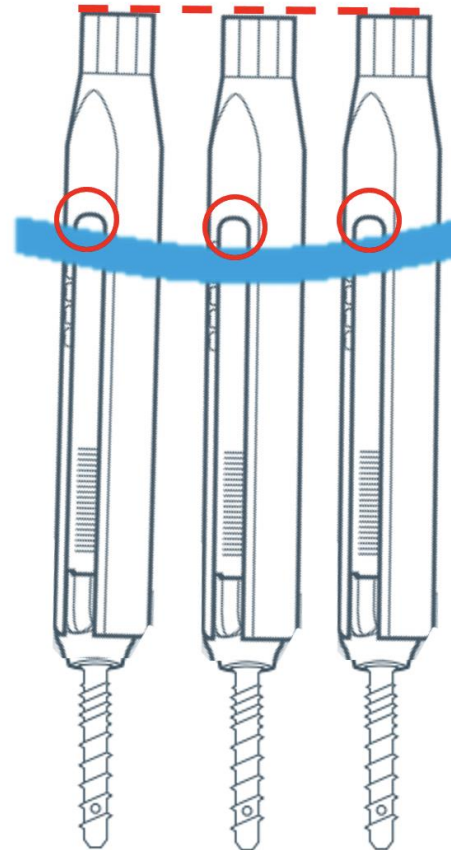
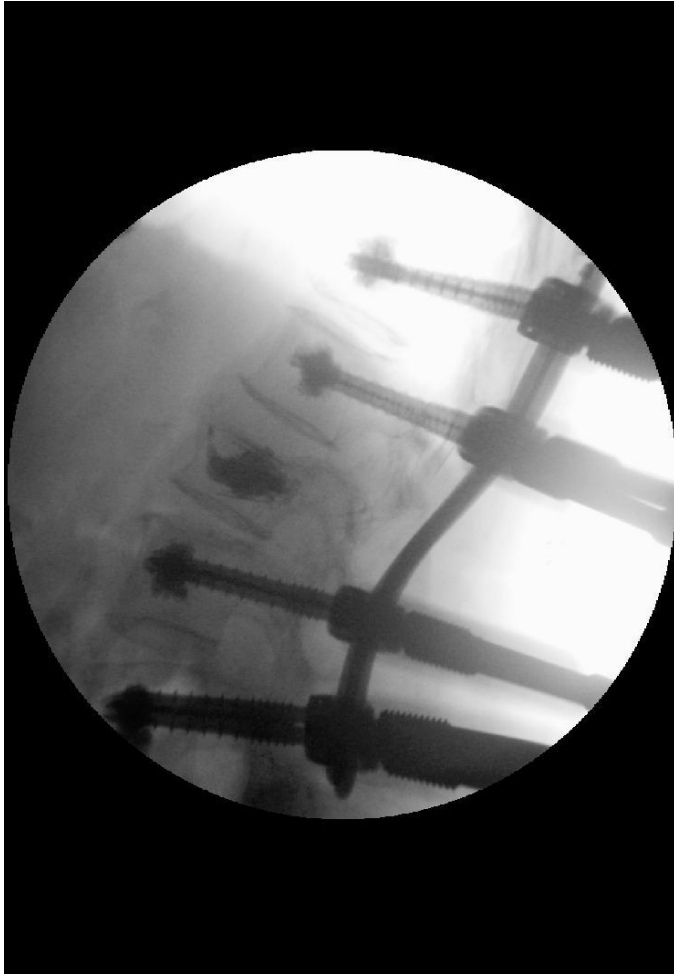




CAD T12 (SJ 5.0mm) with Replacement of the Disc-Material
Temporary: MA-PS T11+L1, PA-PS T10+L2

CR III:

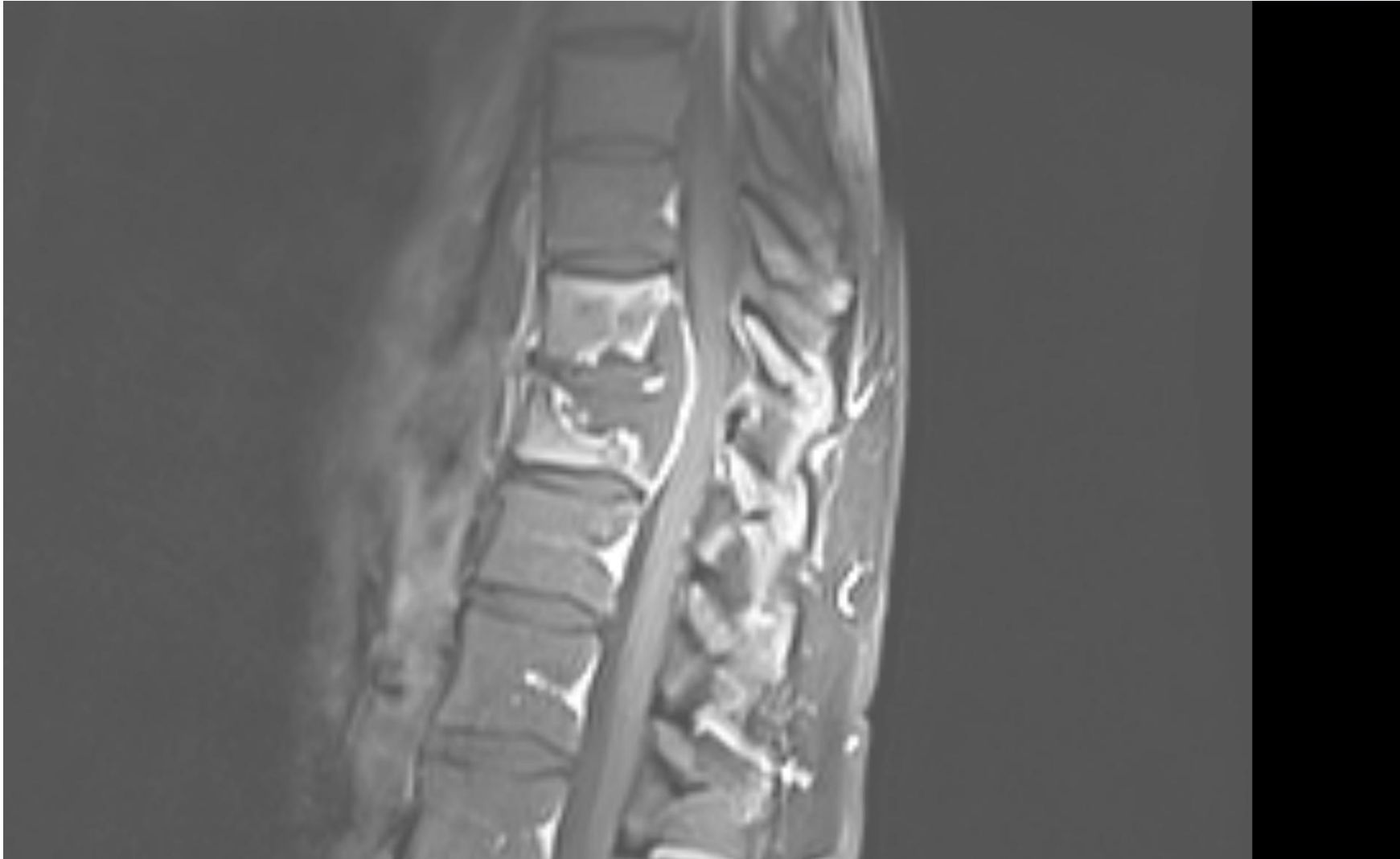
It's all up to the « rod-bending »!!!



CR IV:

Spondylodiscitis T7/8 after difficult cystitis

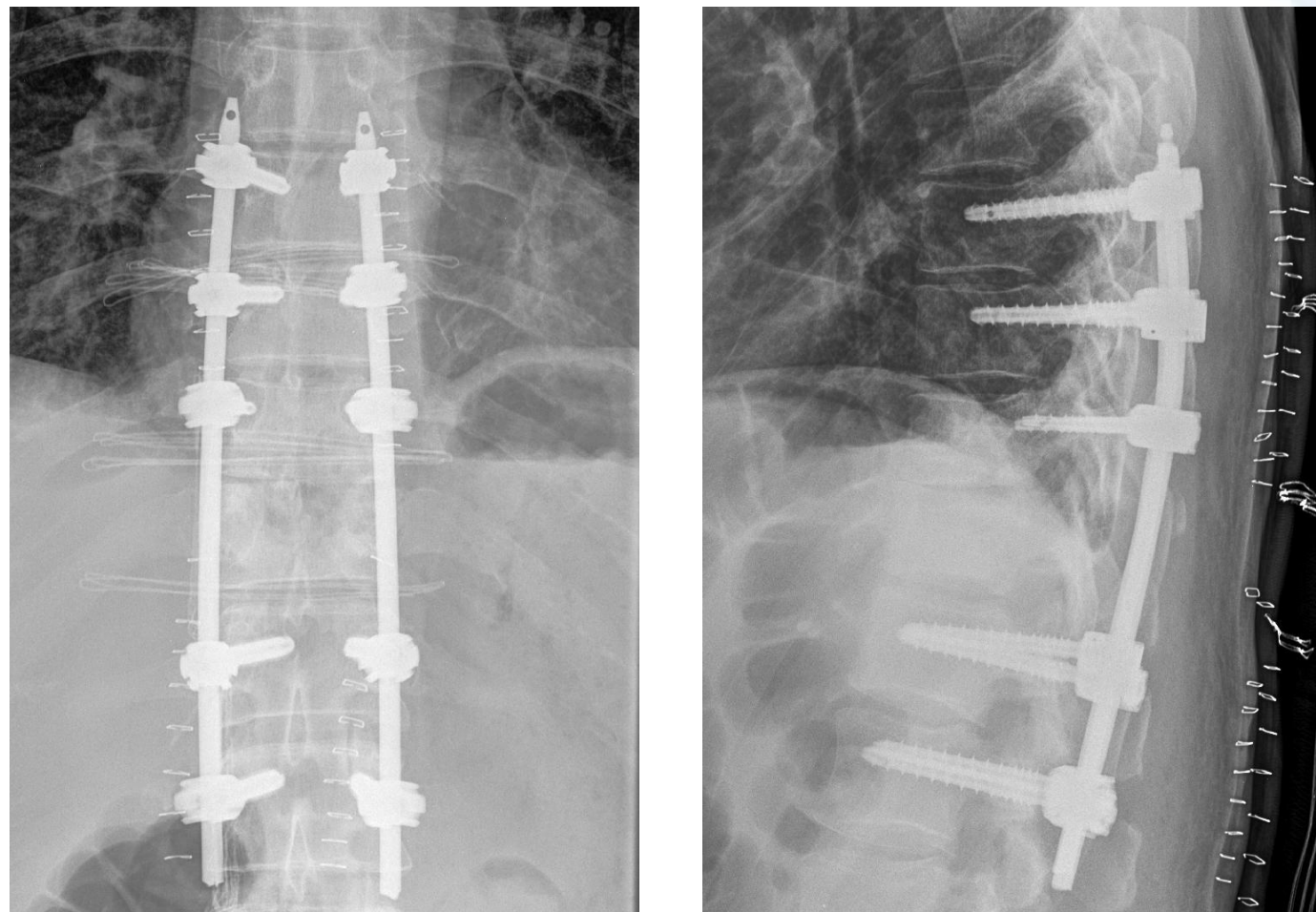
Male, 52 LY, no other secondary diagnosis



Reposition?



But Stability!!!



Perc. Instrumentation T5/6 – T7 (Index!) – T9/10

+

M-Hemilaminectomy T7/8 & Epidural Irrigation

CR V:

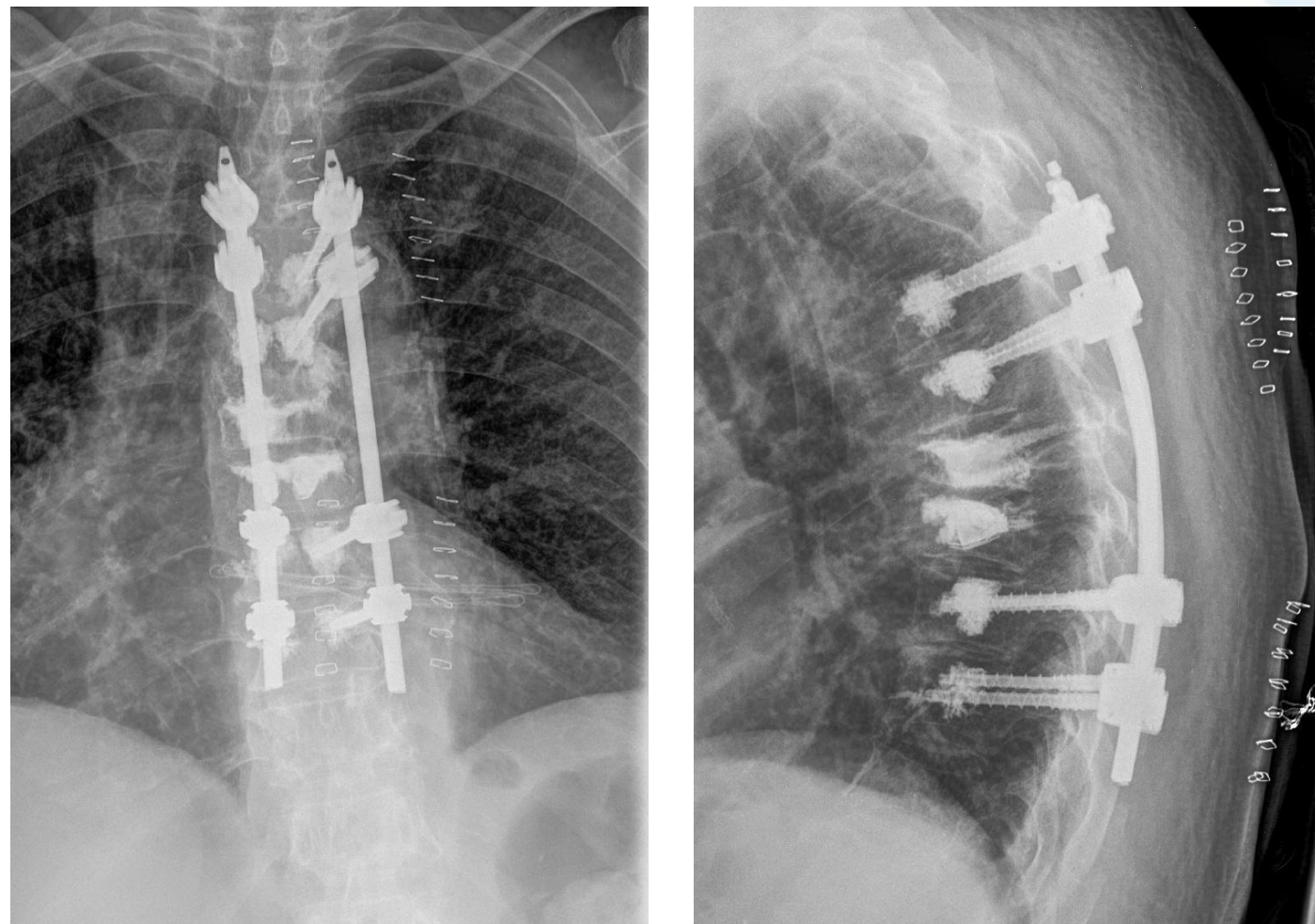
Low-Energy-Trauma, Poor Osteoporotic Bone Qual. (T -3,2)

Female, 77 LY, hpb, coronary heart disease, condition after
extern T7-BKP

Unstable T8-Fracture (AO A4), PF T8 and DP-Fracture T8+9







Hybrid-Tech.: CAD (SJ5.0mm) T8, Perc. Instrumentation T5 PA/6 MA – T9 MA/T10 PA
Zementaugumentation of all PS, Kyphotic Rod Bending

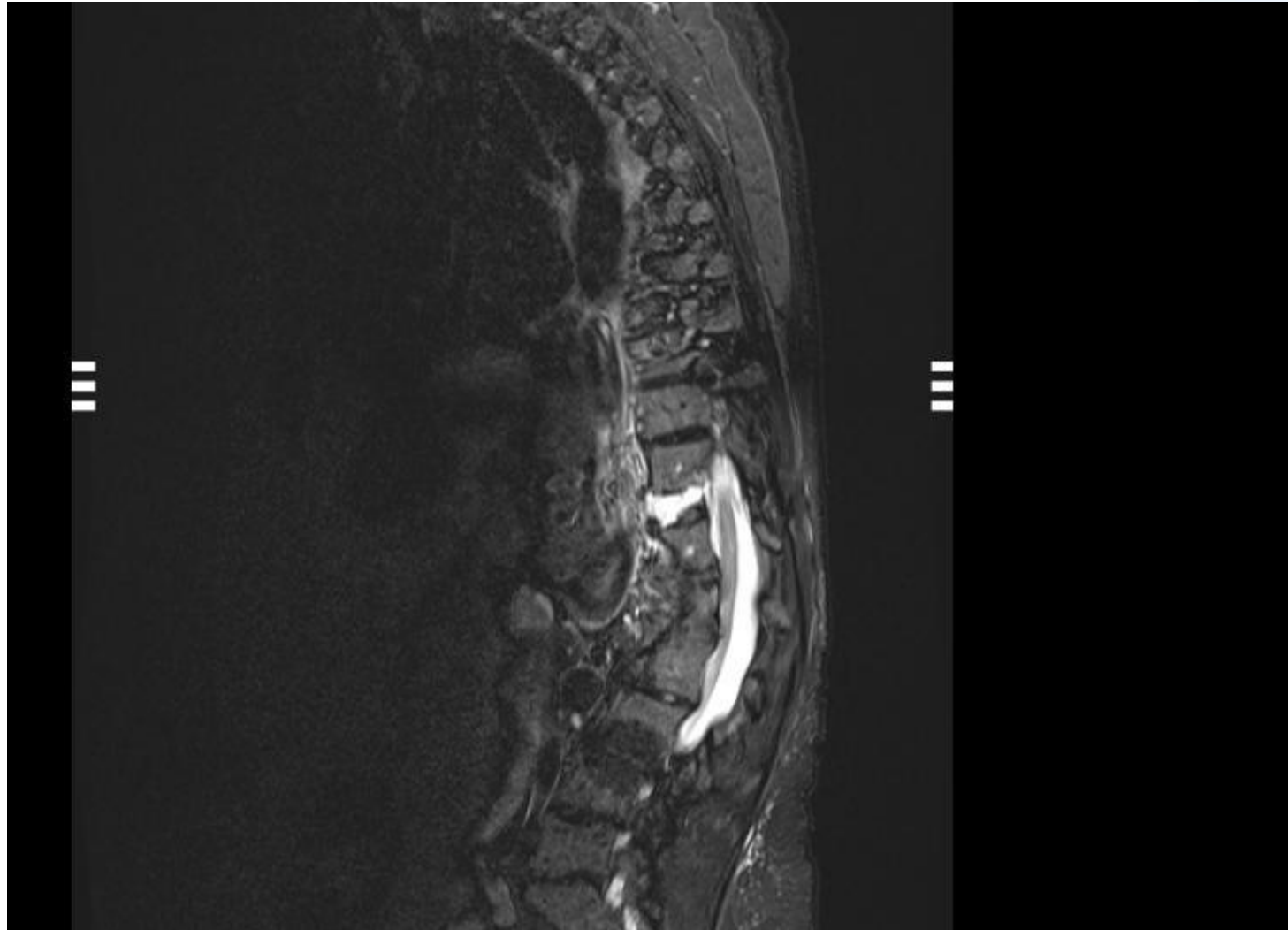
CR V: « THE JURASSIC SPINE »

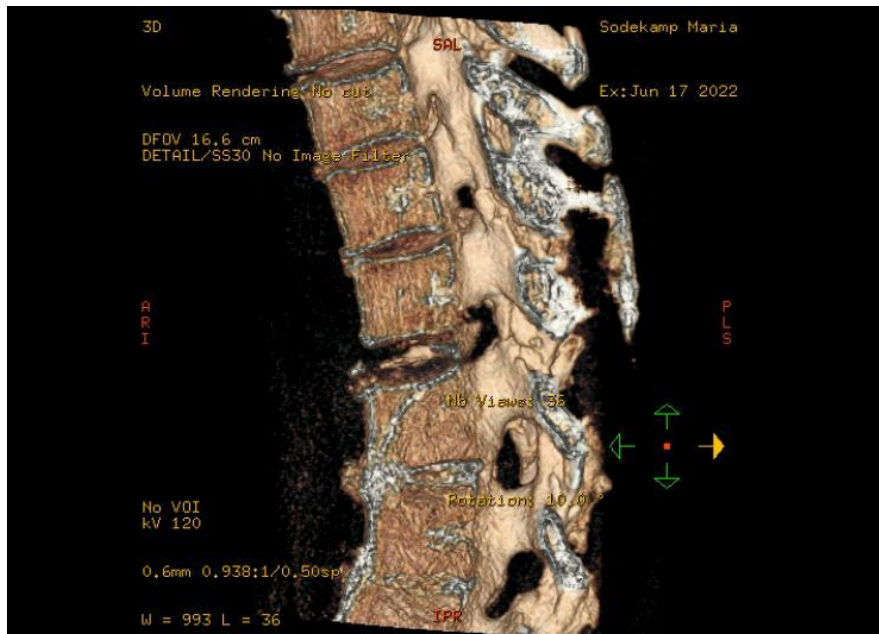
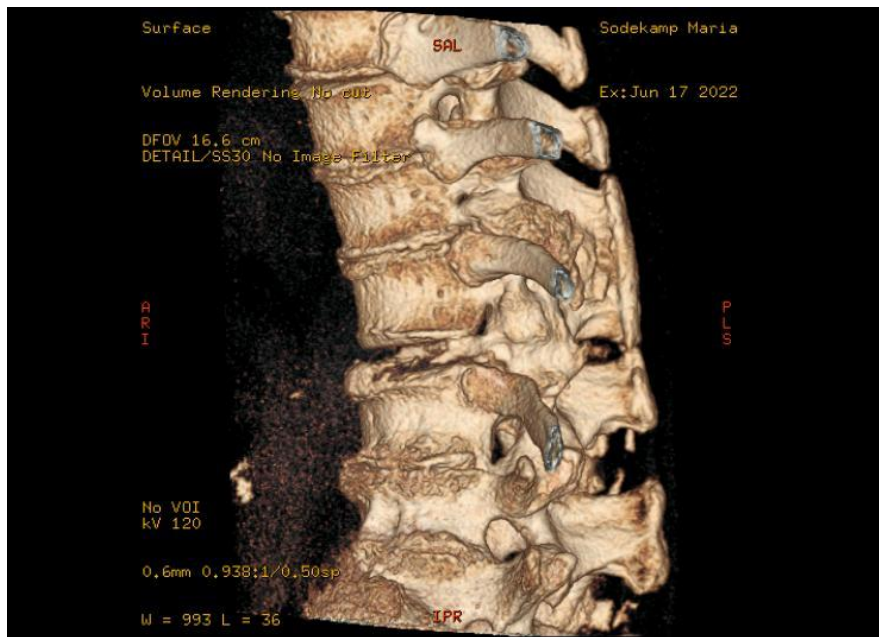
Low-Energy-Trauma, M.Bechterew

Female, 82 LY, severe sec. diagnosis

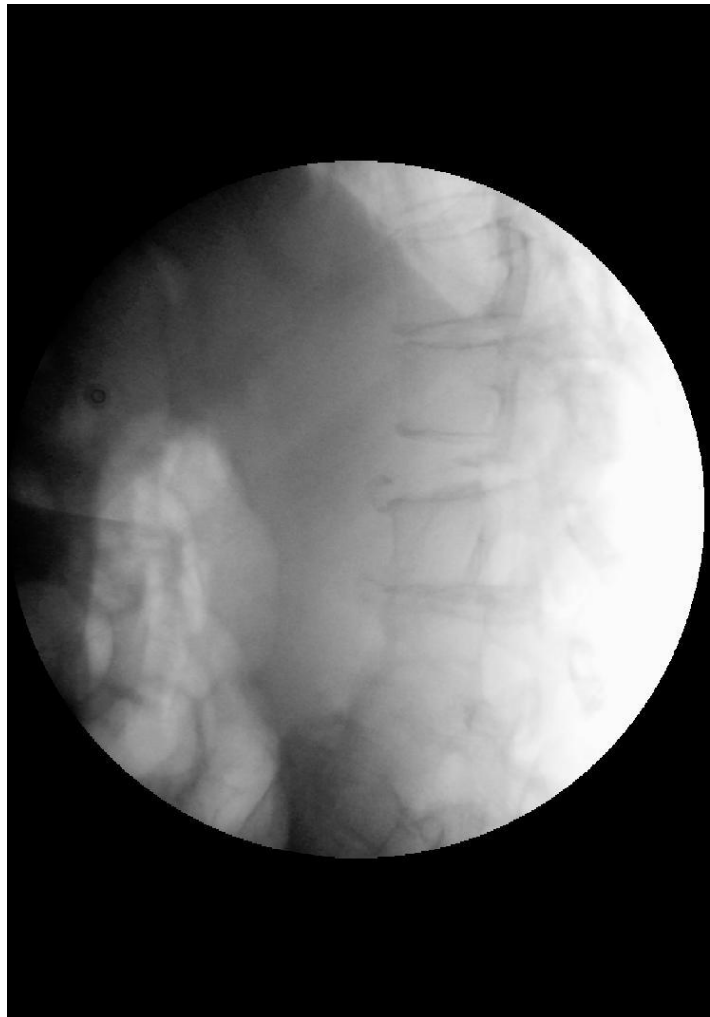
Unstable Gape-Fracture T11/12

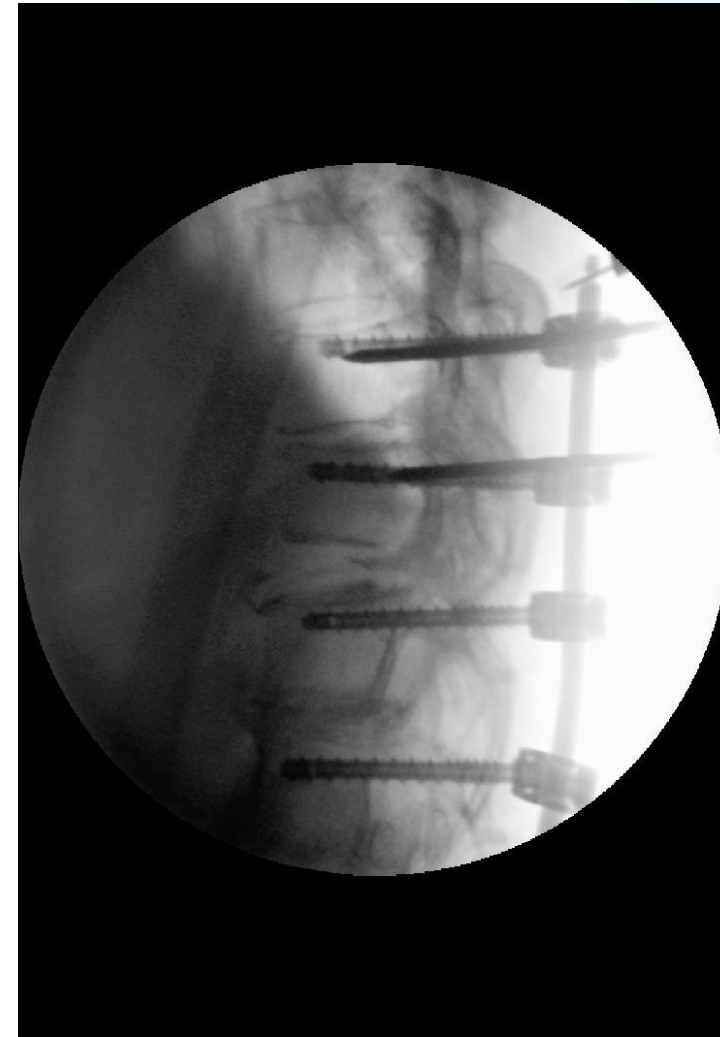
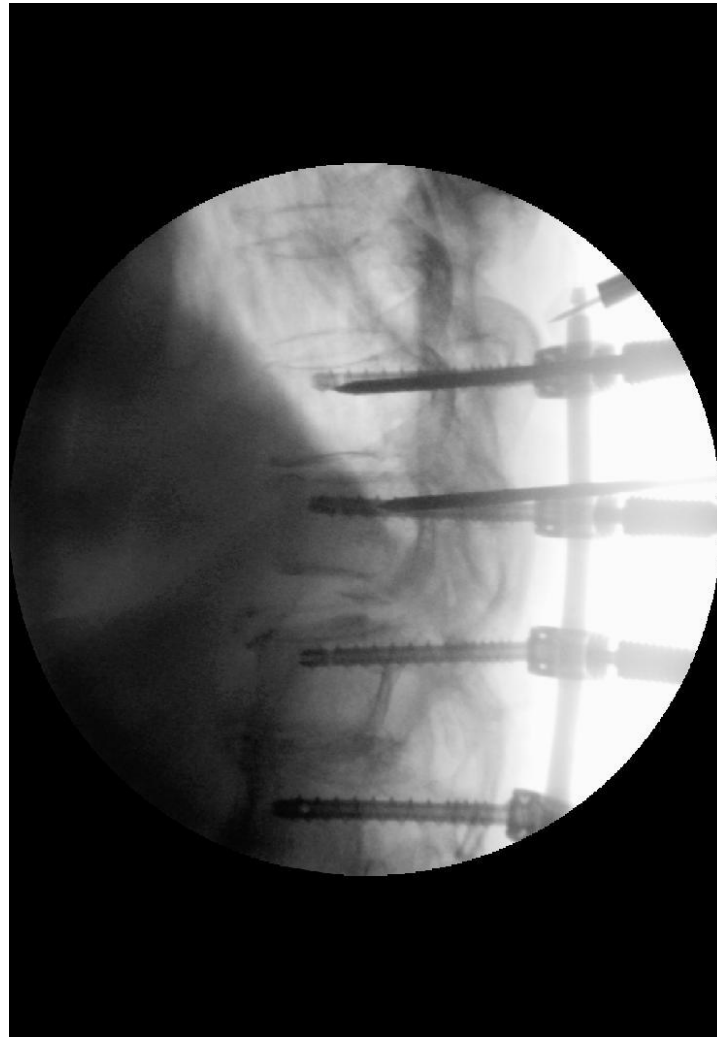




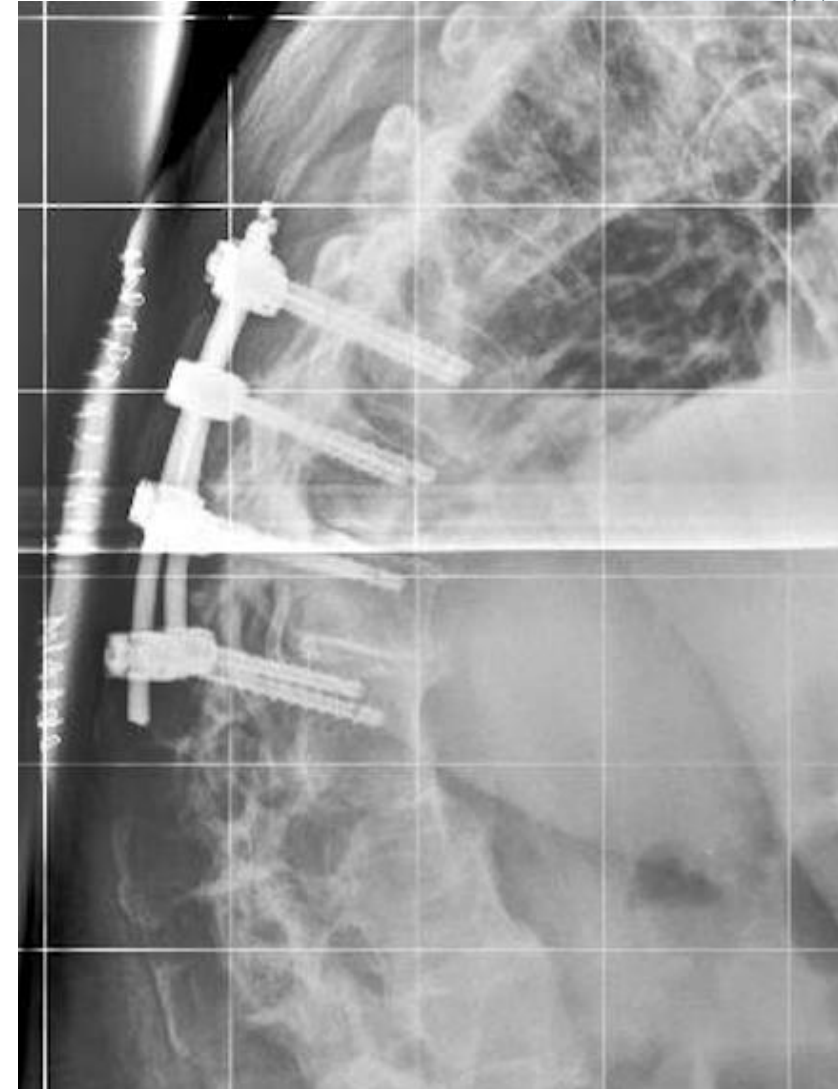














Patrick A. Weidle
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Spine Center
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Mönchengladbach



Thank you for your attention!

